

# A Novel Capacitive-to-Digital Converter Interface Based on MemCapacitors for MEMS Capacitive Sensing Applications

Sondos H.Ismail<sup>1</sup>, Ahmed H.Madian<sup>2,5</sup>, Hassan Mostafa<sup>3,4</sup> and Amr T.Abdel-hamid<sup>1</sup> <sup>1</sup>Electrical and Electronics Engineering Department, German University in Cairo, Egypt.

<sup>2</sup>Engineering Department, National Center for Radiation Research and Technology (NCRRT), Egyptian Atomic

Energy Authority, Cairo, Egypt.

<sup>3</sup>Electronics and Communications Engineering Department, Cairo University, Cairo, Egypt.

<sup>4</sup>Center for Nanoelectronics and Devices, AUC and Zewail City of Science and Technology, New Cairo, Egypt. <sup>5</sup>NISC Research Center, Nile University, Cairo, Egypt.

{sondos.hussein@guc.edu.eg, ahmed.hmadian@gmail.com, hmostafa@uwaterloo.ca, amr.talaat@guc.edu.eg}

Abstract—This paper proposes a new 10-bit fully differential capacitance-to-digital converter (CDC) used in MEMS capacitive sensing applications based on memcapacitors. The proposed digital interface circuit is the voltage based-CDC technique; this achieves a direct physical property (capacitance) conversion into a digital output. The overall proposed design eliminates repeated blocks and can be used independent of the sensor type. The proposed architecture enhances the CDC performance and realizes minimized area due to memcapacitors. A performance comparison between conventional capacitor-based circuit and the circuit using memcapacitors is presented which indicates the same behavior but with an overall huge area reduction and enhanced power consumption. Cadence and LT-SPICE simulations are done using 90nm model with 1V single ended voltage supply. The current consumption at 1 KHz is 5.9  $\mu$ A.

# *Index Terms*—Analog-to-digital converter (ADC), Capacitance-to-digital converter (CDC), MEMS, Memcapacitors.

### I. INTRODUCTION

Successive approximation register (SAR) analog-to-digital converter(ADC) architectures have become the most popular technology for analog/digital conversion interface for all digital signal processing systems [1]. The goal is to acquire the sensed signal with low-power and miniaturized electronic device. Consequently, a numerous number of applications ranging from biomedical, gyroscopes and direction detection to power management applications are in continuous search for low power and low area ADCs for interface conversion purposes [2].

Recently, researchers are targeting the integration of the sensor and the electronic interface circuit together with the least possible area and least power consumption. Capacitive sensing is emerging as a popular interfacing alternative to switches and knobs in different customer electronic devices. It is simply based on the idea of sensing the capacitance electrical property that exists between any two conductive surfaces. Whereas this electric property varies due to the change in a physical property such as: pressure, temperature, position, speed and many other physical properties. There is a variety of capacitive readout circuits and techniques known as capacitance-to-digital

converter (CDC) techniques[3-4]. There are methods including time-based capacitance to digital [5], frequencycapacitance to digital[6]and voltage-based based capacitance to digital converters[7-8]. The most attractive method in terms of power consumption, accuracy and reliability is the voltage-based CDC technique [7-8]. Where the sensed capacitance value is transformed into a digitalized related voltage output. One of the famous CDC architectures is the one proposed by K.Tanakaet al. [7], where a low power single capacitance to digital converter was realized, however, the circuit could not operate at high variation of sensor capacitance frequency. This is due to the dependency of DC level on variation frequency of sensor capacitance. Later in [8] a differential CDC was realized that eliminated the influence of variation of sensor capacitance to the circuit DC level at the output of the capacitor arrays. This can be used further in applications where the sensor value is varied with frequency variations. This differential CDC approach was then reported in variety of applications such as Multisensory systems [9].

In this work, a10-bit fully differential low-power and minimized area capacitance-to-digital converter (CDC) is proposed. This CDC interface circuit is realized using memcapacitors, where the memcapacitor (MemC) behavior and performance characteristics are first studied, and then further the effect of using the memcapacitors is compared with other previous different techniques. The proposed technique can be utilized as a common IC block used after different MEMS sensors to achieve low area and low power on-chip interface system.

The paper is organized as follows: Section II briefly explains the memcapcitor history and theory of operation, followed by the CDC architecture using conventional integrated capacitors in section III. Section IV presents the proposed CDC circuit based on Memcapacitors. Simulation results and comparisons with previous work are included in section V. Finally, the conclusion is stated in section VI.

#### II. MEMCAPACITOR TECHNOLOGY

## A. Introduction

The memory-resistor (known as memristor) was first postulated by Chau in 1971 [10].It remained a postulated idea until HP published the first memristor implementation in 2008 [11].Later in January 2009 the general idea of memory circuit elements was proposed including memcapacitive and meminductive systems as well as their subsystems defined as memcapacitors and meminductors. It would operate in contrast to the memristor, as non-volatile memories with essentially lossless data reading and storing [12].

Memcapacitive system or a memcapacitor can be defined as a passive element whose capacitance is controlled by the amount of electric charge conveyed through it [12]. This charge affects the width of the dielectric. The memcapacitor circuit symbol is shown in Fig.1.



#### Fig. 1 Memcapacitor Circuit Symbol [12].

There are two types of memcapacitive systems: voltagecontrolled and charge controlled systems [13]. According to [12], the charge controlled memcapacitor can be defined from equations (1) and (2), where q(t) is the capacitor charge at time t,  $V_C(t)$  is the corresponding voltage,  $C^{-1}$  is the inverse memcapacitance that depends on the system internal state, and  $\dot{x}$  is the dynamic vector that represents the system internal state variable.

$$V_{C}(t) = C^{-1} * (x, q, t) * q(t)$$
(1)  

$$\dot{x} = f(x, q, t)$$
(2)

Since the above element has gained a great focus in many research areas and fields, a lot of publications and researches were conducted to study the memcapacitor behavior and model it. So, simulation set up was implemented using a SPICE simulation model for the charge-controlled memcapacitor [14]. In these simulations, the memcapacitance value depends on the electric charge that passes through the memcapacitor and its state equation. The state variable x depends on the change of dielectric width L that can vary from  $L_{min}$  to  $L_{max}$  which correspondingly sets a limit range for both minimum and maximum memcapacitances and inverse memcapacitances as shown in equation (3):

$$x = \frac{L - L_{min}}{L_{max} - L_{min}} \in (0, 1) \tag{3}$$

The memcapacitor volt-coulomb pinched hysteresis loop profile is shown in Fig.2. The memcapacitor has the following parameters:  $C_{min}$ =10nF,  $C_{max}$ =10uF,  $C_{int}$ =100nF and driven under 2V-amplitude sinusoidal wave with frequency 1KHz. This is similar to the hysteresis behavior of memristive elements illustrated in [15].

#### III. CDC CIRCUIT ARCHITECTURE

#### A. Circuit Overview

The fully differential CDC circuit is shown in Fig.3. It is composed of a MEMS capacitive sensor  $C_x$ , two exact binary

weighed capacitor arrays (to eliminate the effect of MEMS capacitive sensor variation or fluctuations to output DC level), a scaling capacitor  $C_s$ , a low-voltage comparator, switches and a SAR control logic to generate the final digital code that corresponds to the sensor capacitance value.

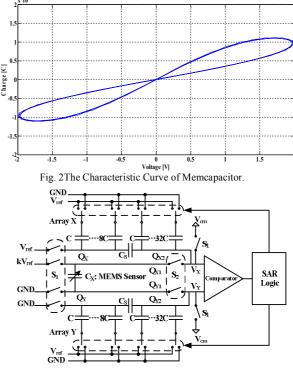


Fig. 3 Conventional CDC Circuit Architecture.

#### B. Operation of the Differential CDC

The CDC has two modes of operation: the sampling mode and the conversion mode; where both are based on a binary search algorithm and charge redistribution architecture.

In the first phase, switch  $S_1$  is turned on; switch  $S_2$  is turned off and switches of bottom plates of capacitor arrays X and Y are connected to  $V_{ref}$  and ground, respectively.

In the second phase, switch  $S_1$  is turned off and switch  $S_2$  is turned on. The conversion mode begins with the most significant bit conversion (MSB).First, the MSB switch of capacitor array X is connected to ground and all other switches in the array remain connected to  $V_{ref}$ . Whereas in array Y, all switches are connected opposite to array X. Due to the charge redistribution and the law of charge conservation in both capacitor arrays X and Y, the voltage at the input nodes of the comparator is:

$$|V_X - V_Y| = 2 * \frac{C_{MSB} - \kappa C_X}{2C_X + C_{UPPER} + \frac{C_S C_{LOWER}}{C_S + C_{LOWER}}} * V_{REF}(4)$$

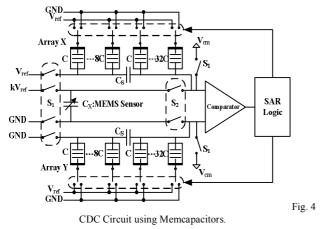
Where  $C_{MSB}$  is the MSB capacitance,  $C_{UPPER}$  is the total capacitance of the upper bits capacitor array at the right side of the scaling capacitor  $C_S$ , k is a scaling factor and  $C_{LOWER}$  is the total capacitance of the lower bits capacitor array at the left side of the scaling capacitor  $C_S$ . The voltages  $V_X$  and  $V_Y$  are compared mutually and the comparator output determines which input voltage is at

higher level. Accordingly comparing voltages  $V_X$  and  $V_Y$  means comparing  $C_{MSB}$  and  $kC_X$ . If  $C_{MSB}$  is smaller than  $kC_X$ , the MSB is kept "1" and the MSB switch of array X and Y is kept connected to  $V_{ref}$  and ground, respectively. Else, the MSB switch is set to "0" and the MSB switch of array X and Y is reset to ground and  $V_{ref}$  respectively. When the conversion of MSB is finished, conversions of the next bits are carried out one by one in the same process described until the least significant bit (LSB), to reach a differential voltage approaching0. Finally, the output digital code indicates the most nearest approximated value of the capacitive sensor value.

#### IV. CDC CIRCUIT USING MEMCAPACITORS

In this paper, the CDC circuit is realized replacing the binary weighted conventional integrated capacitors by memcapacitors. The study started by replacing one capacitor in each array at a time to study the effect of the memcapacitor on the response of the CDC circuit. The memcapacitor model used is the SPICE model indicated in [14]. To replace a normal integrated capacitor by a memcapacitor, the value of the memcapacitor is determined by fixing both values  $C_{min}$  and  $C_{int}$  and only changing the value of  $C_{max}$ .

Fig.4 shows the CDC architecture after replacing all conventional capacitors by memcapacitors.



#### V. SIMULATION RESULTS

Simulations are done using CADENCE and LT-SPICE tools, where the MEMS sensor capacitance value is varied in the range of pF. The comparator used is realized in CMOS architecture using 90 nm transistor model. The MEMS capacitive pressure sensor is first studied and simulated using COMSOL multi-physics tool to study its behavior, and then the variation in the sensor's capacitance is modeled in CADENCE and LT-SPICE tools.

Fig.5 shows the simulation results of the CMOS comparator input voltages  $V_x$  and  $V_y$  first using conventional integrated capacitors setting the capacitance sensor value to 3pF, the conversion frequency was around 10KHz. Simulation result shows that these two voltages are symmetric around the common voltage  $V_{cm}$ =0.5v which is the output of the capacitor arrays.

Also, Fig.5shows the output voltages at the capacitor arrays, after replacing the conventional integrated capacitors with memcapacitors. The simulation results show that the CMOS comparator input voltages are symmetric too around  $v_{cm}$ =0.5v.

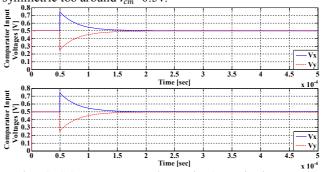


Fig. 5 CDC Comparator Input Voltages using Conventional Integrated Capacitors and Memcapacitors.

The results show that the CDC circuit performance using memcapacitors and conventional integrated capacitors are almost the same, yet the use of memcapacitors greatly reduces the design area.

Fig.6 shows the conversion results of the MEMS capacitive pressure sensor using the proposed memcapacitor based CDC architecture. In which the capacitance of the MEMS sensor is varied in the pF range and the digital output code is converted into its decimal equivalent.

In[16], a memristor was realized using a TiO<sub>2</sub> thin film sandwiched between two metal plates where the total area of this model was measured to be in the range of (500 nm<sup>2</sup>to 2500 nm<sup>2</sup>). In[17], a memcapacitor realization was presented where a memcapacitor can also be fabricated using a TiO<sub>2</sub> thin film sandwiched between two metal plates which is similar to the approach used for the memristor presented in[16].As a result, a memcapacitor area can be estimated to be in the nm<sup>2</sup> range (10<sup>-18</sup>m<sup>2</sup>).So unlike the conventional capacitor where the MOSFET realization depends on C<sub>OX</sub> of the MOSFET[18]as shown in the equations below:

$$C_{eff} = C_{OX} * W * L + 2 * C_{ol} * W(5)$$

The smallest value for the capacitor used in this paper is 1 pF that requires an area of  $81.1 \ \mu m^2$  for 90nm CMOS technology, which is highly greater than the area of memcapacitor. Table 1shows the area values of the conventional integrated capacitors with different values of capacitance compared to the estimated area of the memcapacitor as indicated in [17]. The value of thememcapacitor depends on the biasing as shown earlier in the memcapacitor section; therefore the memcapacitor area is fixed regardless of its value as shown in Table 1.

Finally, Table 1 clearly shows the great area reduction due to replacing the conventional integrated capacitors with memcapacitors. This massive area reduction is a very attractive feature for different applications including biomedical applications where the area is the main factor in implanted devices.

An overall performance comparison between the proposed CDC architecture and previous architectures is presented in Table 2.

TABLE I MEMCAPACITORS AND CONVENTIONAL INTEGRATED CAPACITORS AREA COMPARISON

Capacitance Value	Conventional Integrated Capacitor Area	Memcapacitor Area					
1 pF	81.1 μm <sup>2</sup>	$(0.0005 \mu m^2 to 0.0025 \mu m^2)$					
2 pF	$162.2 \ \mu m^2$						
4 pF	324.4µm <sup>2</sup>						
8 Pf	648.8µm <sup>2</sup>						
16 pF	1297.6µm <sup>2</sup>						
32 pF	2595.2µm <sup>2</sup>						
00 00 00 00 00 00 00 00 00 00	20 30 40 50						
Input Sensor Capacitance [pF]							
Fig. 6Conversion Results of the proposed Memcapacitor CDC.							

TABLE 2 PROPOSED CDC CIRCUIT OVERALL PERFORMANCE COMPARISON

Specifications	Tanaka [7]	Vo [8]	Lai [5]	This Work
Technology	180nm	180nm	180nm	90nm
Power Supply	1.4 V	1.4 V	1.8 V	1 V
Resolution (ENOB)	8 Bit (6.83)	10 Bit	(6.7)	10 Bit (9.3)
Power/Current Consumption	360µA	29.7μΑ	82μW/45.6 μA	5.9 μΑ
Area	0.034 mm <sup>2</sup>	0.11 mm <sup>2</sup> (estimated)	0.0354 mm <sup>2</sup>	$\begin{array}{c} 0.0005 \mu m^{2}t\\ o\ 0.0025\\ \mu m^{2}\\ (estimated\\ for\ each\\ MemC) \end{array}$
Conversion Frequency	262 KHz	262 KHz	125 KHz	10 KHz

#### VI. CONCLUSION

A new realization for a fully differential 10-bit capacitanceto-digital converter for MEMS capacitive sensors based on memcapacitors was proposed. The conventional integrated capacitors in the capacitor arrays were replaced by memcapacitors. The design was realized in 90nm CMOS technology under 1V single ended voltage supply for different capacitive sensor applications. The realized converter achieved an Effective Number of Bits (ENOB) of 9.3band SNR of 57.75 dB. The use of the memcapacitor instead of the conventional integrated capacitors reduced the overall area of the circuit dramatically, while maintaining a similar response to that of the conventional integrated capacitor. The proposed technique thus achieved the best of both technologies MEMS and Memcapacitors by combining them together. This enhances the digital signal processing circuit when it is integrated in any MEMS capacitive sensor system independent of the number of sensors or their types. Thus, makes it more suitable for biomedical applications, wireless sensor networks and direction detection applications.

#### VII. REFERENCES

- F. Chen, A. P. Chandrakasan and V. Stojanovic, "A Low-power Area-efficient Switching Scheme for Charge-sharing DACs in SAR ADCs," *Custom Integrated Circuits Conference (CICC)*, pp. 1-4, Sept. 2010.
- [2] C. Yuan and Y. Lam, "An ultra-low Energy Capacitive DAC Array Switching Scheme for SAR ADC in Biomedical Applications," *International Conference on IC Design & Technology (ICICDT)*, pp. 1-4, May 2011.
- [3] H. Ha, D. Sylvester, D. Blaauw and J. Sim, "A 160nW 63.9fJ/conversion-step Capacitance-to-Digital Converter for Ultra-Low-Power Wireless Sensor Nodes," *IEEE International Solid-State Circuits Conference (ISSCC)*, pp. 220-221, Feb. 2014.
- [4] S. Xia, K. Makinwa and S. Nihtianov, "A Capacitance-to-Digital Converter for Displacement Sensing with 17b Resolution and 20us Conversion Time," *IEEE International Solid-State Circuits Conference (ISSCC)*, pp. 198-199, Feb. 2012.
- [5] K. Lai, Z. He, Y. Yang, H. Chang and C. Lee, "A 0.0354mm2 82uW 125K/s 3-Axis Readout Circuit for Capacitive MEMS Accelerometer," *IEEE Asian,Solid-State Circuits Conference (A-SSCC)*, pp. 109-112, Nov. 2013.
- [6] H. Danneels, K. Coddens and G. Gielen, "A Fully-Digital 0.3V, 270nW Capacitive Sensor Interface Without External References," *IEEE European Solid-State Circuits Conference (ESSCIRC)*, pp. 287-290, Sept. 2011.
- [7] K. Tanaka, Y. Kuramochi, T. Kurashina, K. Okada and A. Matsuzawa, "A 0.026mm2 Capacitance-to-Digital Converter for Biotelemetry Applications Using a Charge Redistribution Technique," *IEEE Asian ,Solid-State Circuits Conference, (ASSCC),* pp. 244-247, Nov. 2007.
- [8] T. Vo, Y. Kuramochi, M. Miyahara and T. Kurashina, "Asynchronous Differential Capacitance-to-Digital Converter for Capacitive Sensors," Synthesis and System Integration of Mixed Information Technologies (SASIMI), Mar. 2009.
- [9] H. Jiang, Z. Wang, L. Liu, C. Zhang and Z. Wang, "A combined Low Power SAR Capacitance-to-Digital/Analog-to-Digital Converter for Multisensory System," *Midwest Symposium on Circuits and Systems* (MWSCAS), pp. 1000-1003, Aug. 2012.
- [10] L. Chua, "Memristor-The missing circuit element," *IEEE Transactions on Circuit Theory*, vol. 18, no. 5, pp. 507-519, Sept. 1971.
- [11] D. Strukov, G. Snider, D. Stuwart and R. Williams, "The Mising Memristor Found," *Nature*, vol. 453, pp. 80-83, May 2008.
- [12] M. Ventra, Y. Pershin and L. Chau, "Circuit Elements with Memory: Memristors, Memcapacitors, Meminductors," *Proceedings of the IEEE*, vol. 97, pp. 1717-1724, Oct. 2009.
- [13] D. Biolek, Z. Biolek and V. Biolkova, "SPICE Modeling of Memristive, Memcapacitive and Meminductive Systems," *Proceedings International European Conference on Circuit Theory* and Design (ECCTD), pp. 249-252, Aug. 2009.
- [14] D. Biolek, Z. Biolek and V. Biolkova, "SPICE Modeling of Memcapacitor," *Electronics Letters*, vol. 46, no. 7, pp. 520-522, Apr. 2010.
- [15] A. S. Elwakil, M. E. Fouda and A. G. Radwan, "A Simple Model of Double-Loop Hysteresis Behavior in Memristive Elements," *IEEE Transactions on Circuits and Systems II*, vol. 60, no. 8, pp. 487-491, Aug. 2013.
- [16] M. Hu, H. Li, X. Wang and R. Pino, "Geomtry Variations Analysis of TiO2 Thin-Film and Spintronic Memristors," Asia and South Pacific Design Automation Conference (ASP-DAC), pp. 25-30, Jan. 2011.
- [17] A. Bratkovski and R. S. Williams, "Memcapacitor". United States Patent US 2012/0039114 A1, 16 Feb. 2012.
- [18] R. Fan, J. Xu and X. Wu, "A MOSFET-Only Delta-Sigma Modulator for Implantable Neural Signal Sensors," *Proceedings of the International Multiconference of Engineers and Computer Scientists* (IMECS), vol. II, pp. 1282-1285, Mar. 2010.